

# Scaling (II)

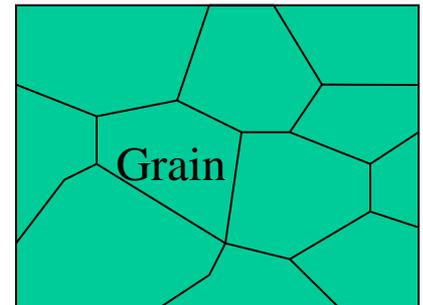
# Scaling in material properties

( Elastic modulus, Poisson's ratio, fracture strength, yield strength, residual in-plane stress, conductivity, .. )

The properties of thin-film material are often different from their bulk / macroscopic form. The disparity arises from

- The different fabrication processes

- ▶ Macroscale: casting, machining, milling, cutting, 3D printing
- ▶ Microscale: deposition (single-crystal, amorphous) , etching, ..



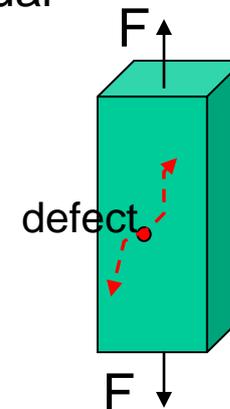
- The assumption of homogeneity

- ▶ Macroscale: usually is accurate
- ▶ Microscale: unreliable when used to model devices that have dimensions on the scale of individual grains

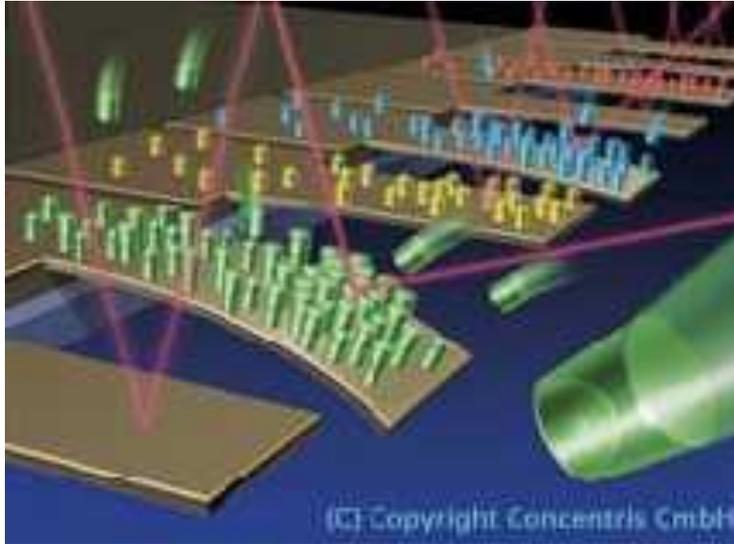
- The defect density

- ▶ Macroscale: high defect counts
- ▶ Microscale: low defect counts

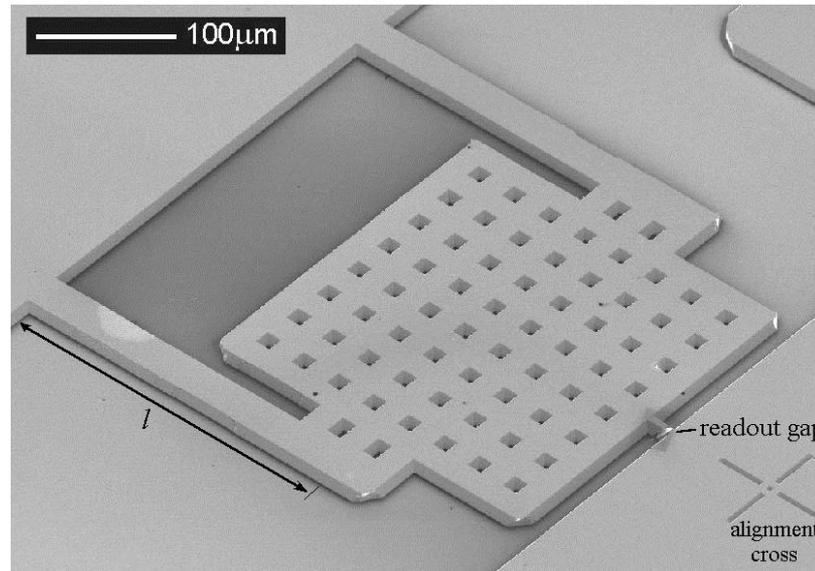
$$\# \text{ defects} = D_{\text{defect}} * \text{Volume}$$



# ■ Scaling in a mechanical system (e.g. a cantilever beam)

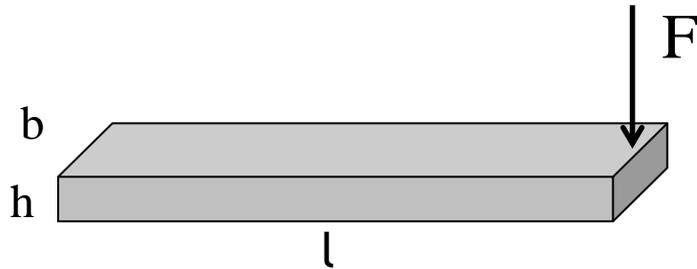


Cantilever biosensor



Cantilever accelerometer

- Stiffness of a cantilever



$$k \approx \frac{\text{force}}{\text{deflection from equilibrium}}$$

$$k = \frac{EI}{l^3}$$

l: area moment of inertia around the end of the beam

$$k \gg E \frac{b \times h^3}{l^3} \sim L^1$$

E is the elastic modulus of the spring material

## Implications ?

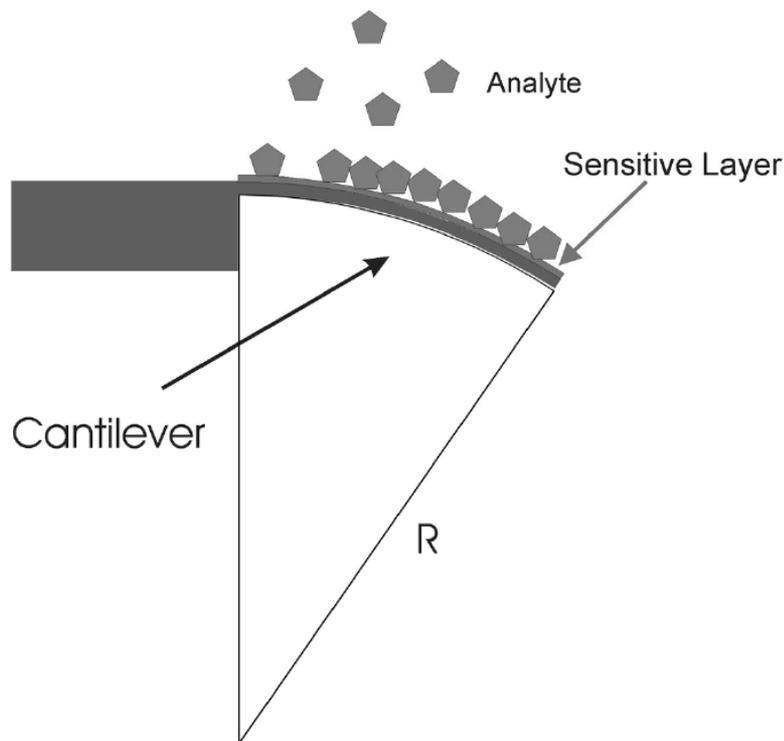
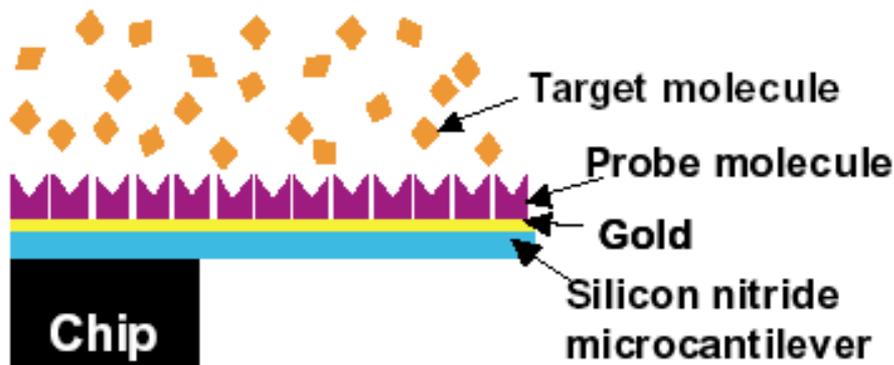
Displacement  $x = F / k$  ;

$$F = m \cdot a \sim L^3$$

$x \sim L^2$  ( a beam of 10-fold smaller in size has 100-fold smaller deflection under a same acceleration)

- (+) A micro accelerometer can experience more than 100,000 g
- (-) for the devices requiring proof mass (e.g. accelerometer) must have a highly sensitive motion-detection signal-transduction system

- Cantilever as biosensors



In **static mode detection**, the deflection of individual cantilever depends on the stress induced by binding reaction of the specific compounds to the interface. Typically, the cantilever surface is coated with a metallic layer (Au) and subsequently activated by binding a receptor molecule directly via a thiol group to the interface.

### Stoney's Law

$$\sigma = Et^2[6R(1 - \gamma)]^{-1}$$

$\sigma$ : stress

R: Radius of the curvature

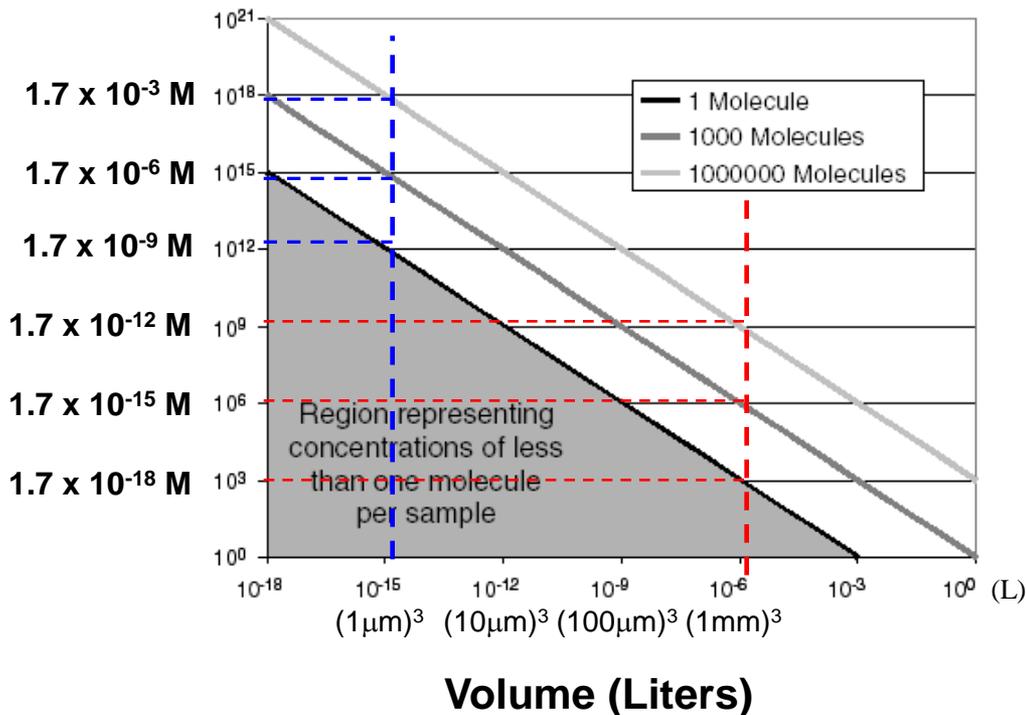
E: Young's modulus

$\gamma$  : Poisson ratio

T: thickness of the cantilever

$$R = \frac{Et^2}{6\sigma(1 - \gamma)} \sim t^2$$

# Scaling in a chem/biological system



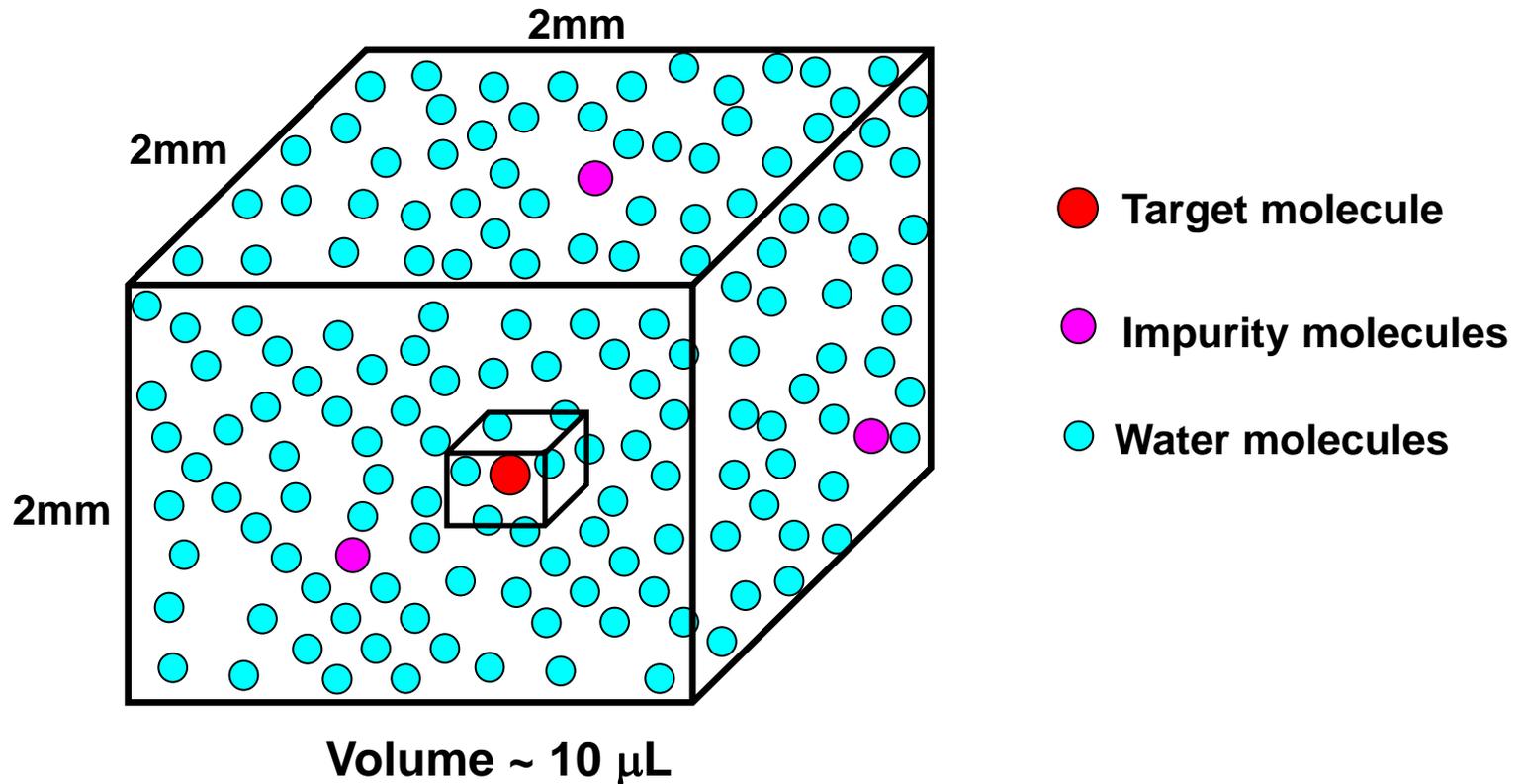
- Volume
- Concentration
- Sensitivity

Volume	1 $\mu$ l	1nL	1pL	1fL	1aL
# of molecules in 1 $\mu$ M solution	6x10 <sup>11</sup>	6x10 <sup>8</sup>	6x10 <sup>5</sup>	600	0.6

- Low volume requires a sensing method with higher sensitivity
- Measurement with extremely low volume enables single-molecule measurement at the physiological concentration level

## Scaling in a chem/biological system (cont.)

- Noise Reduction by Downscaling Detection Volume



**$10^{20}$  excess background molecules over 1 target molecule**

## ■ Scaling in a thermal system

- ◆ Thermal mass (thermal capacity)

$$M \cdot C_p \sim L^3$$

$C_p$  : specific heat

- ◆ Heat transfer

- Heat conduction rate  $Q = -kA \frac{\Delta T}{\Delta x} \sim L^1$

k: thermal conductivity

A: area

T: temperature

x: distance

- Heat convection rate  $Q = qA = hA\Delta T \sim L^2$       h: heat transfer coefficient

***Thermal capacity will scale down more rapidly than heat transfer***

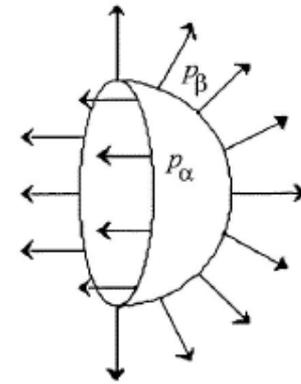
- A more careful analysis is required to predict the thermal behavior of miniature structure when they are scaled down to sub-micro dimensions. The dimensions are of the same scale as the quantum mechanical ***phonon***, or ***quantum of lattice vibration***

# Scaling in surface tension

▶ Surface tension force =  $\gamma \cdot L \sim L^1$

**Example** : Surface tension ( $\gamma_{\text{water}} \sim 72 \text{ mN/m}$ )

- A bug (10 mg) needs 1 mm of foot edge to walk on water
- A human (60 kg) would need feet with 8000 m to walk on water



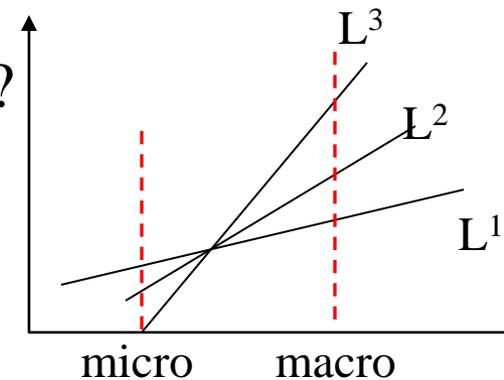
**Figure 1.** Imaginary hemispherical section of a spherical liquid drop. The arrows pointing radially outwards represent forces due to the pressure difference ( $p_\alpha - p_\beta$ ). The arrows pointing to the left represent forces due to surface tension.

$$\Delta P = \gamma \left( \frac{1}{R_1} + \frac{1}{R_2} \right) \sim L^{-1}$$

- 20  $\mu\text{m}$  hydrophilic channel filled with water,  $\Delta P$  across meniscus is 12.5 kPa

▶ What are the implications for micro devices ?

- Stiction problems during releasing structures
- Surface-tension related forces becomes effective



# The Lotus Effect

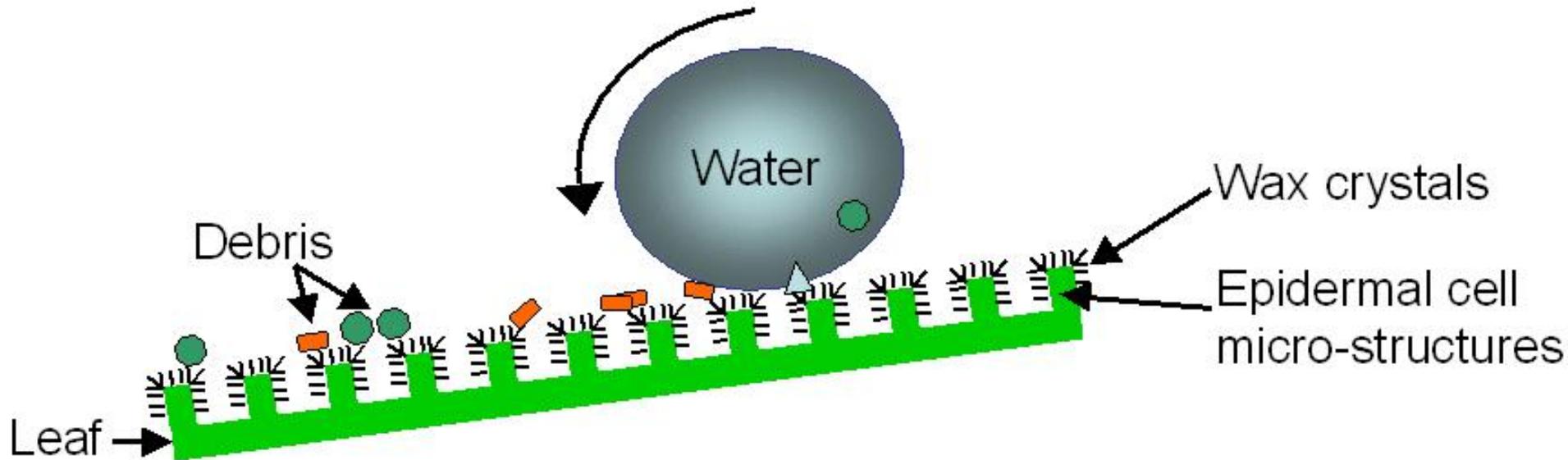
Lotus leaves and nasturtium leaves are self-cleaning due to nano and microscale structures and a waxy coating.

Together these features create a superhydrophobic surface.

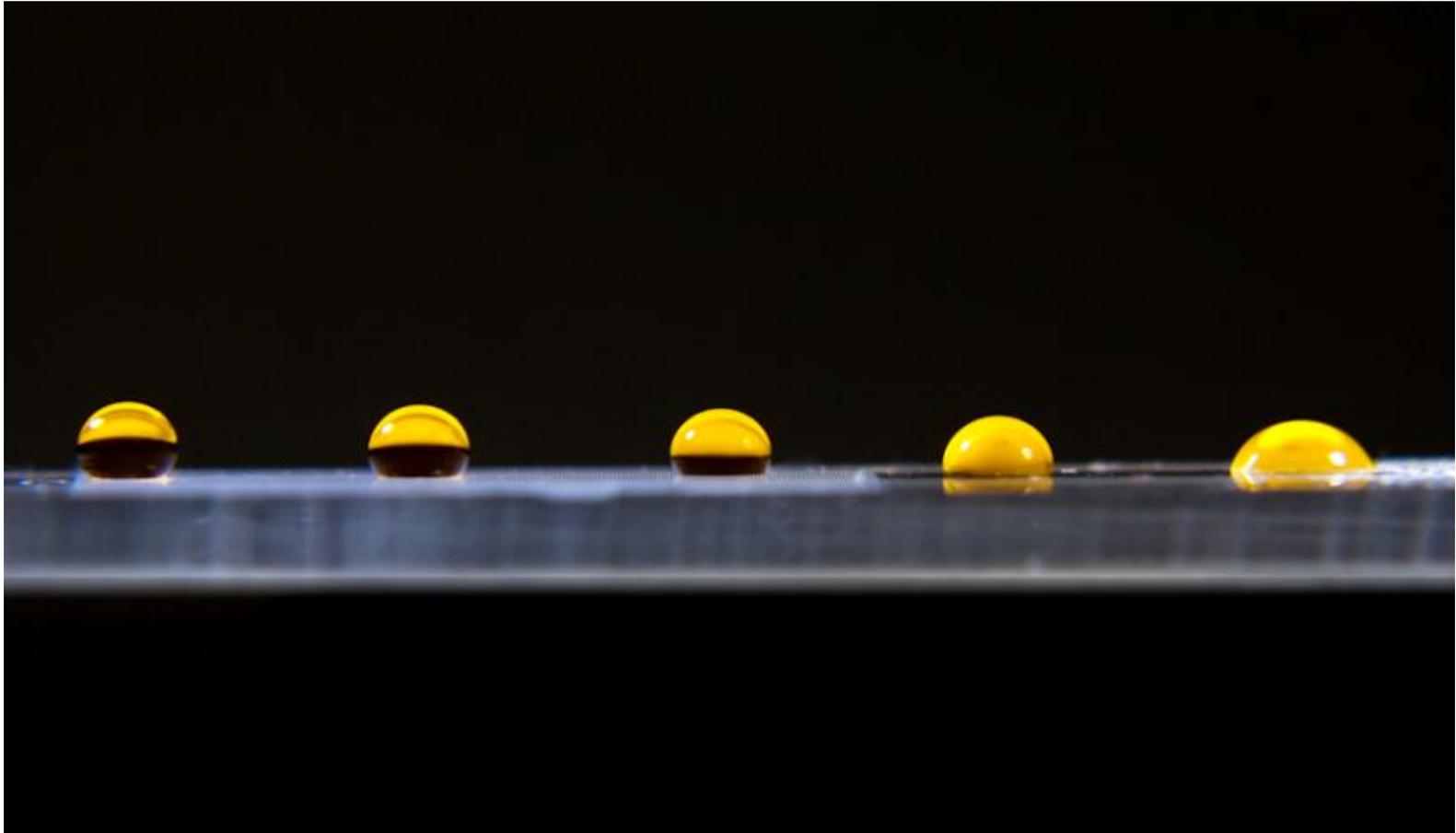


Close-up of a nasturtium leaf, which exhibits the **Lotus Effect**, with a droplet of water

# The Lotus Effect



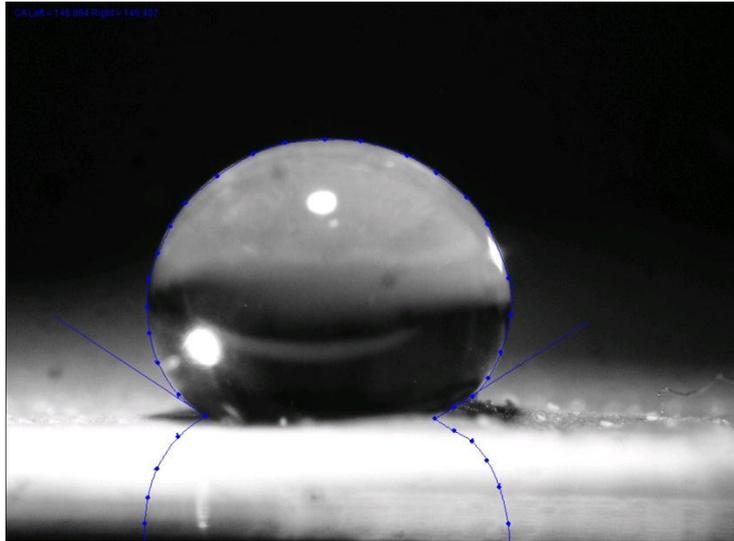
# Droplet “Digital Microfluidic” Technology



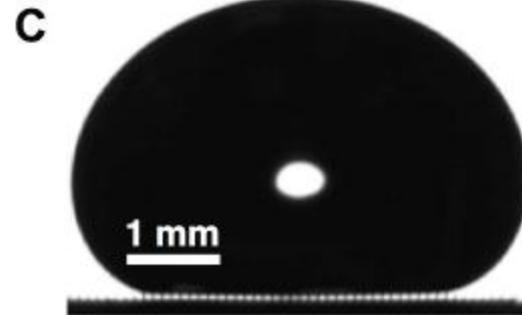
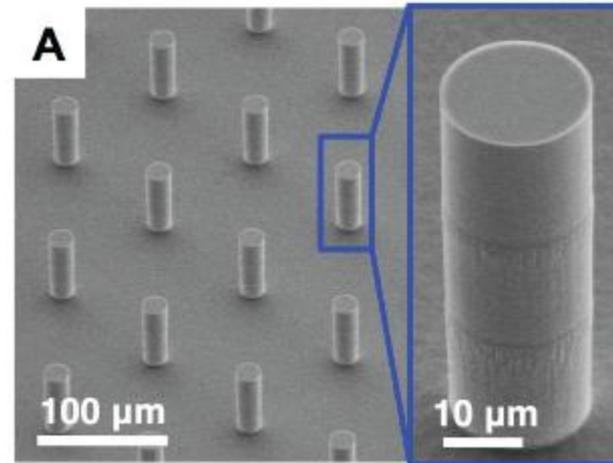
(Photo by Y Zhang & C Beh)

**Grand Prize Winning Photo, 2013 JALA & JBS Art of Science Contest**  
Society of Laboratory Automation and Screening (slas)

# ■ Superhydrophobicity



A water drop on a lotus surface showing contact angles of approximately  $147^\circ$  .



A water drop on an array of silicon micro posts showing contact angles of approximately  $160^\circ$  .

## ■ Scaling in friction

### ▶ The sources of friction

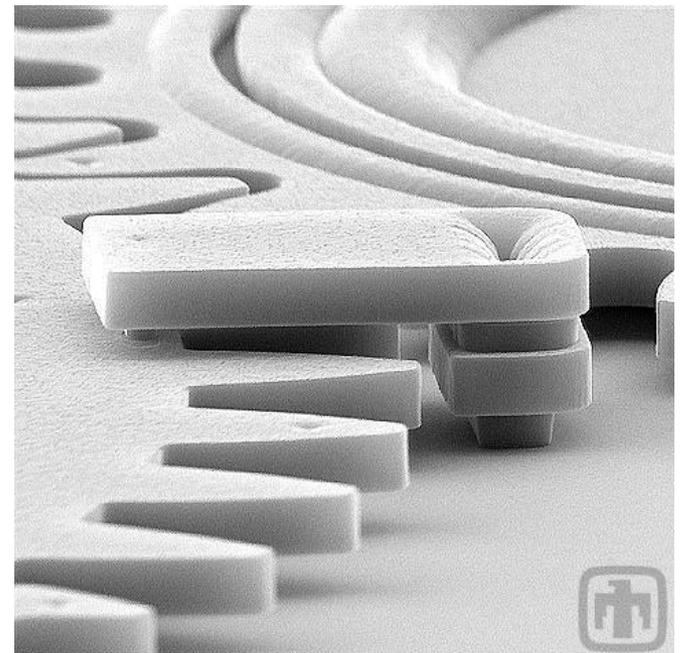
- Capillary forces  $\sim L^1$
- Adhesive surface forces such as van der Waals, hydrogen bonding, electrostatic  $\sim L^2$

### ▶ Surface roughness vs friction

- Macroscale contact occurs between few rough protrusions
- When the surface is well polished and becomes highly smooth, the contact occurs over larger area

### ▶ Friction in MEMS

- To suspend structure or dimple to avoid or reduce friction



# Scaling in diffusion

- Diffusion times (particle and thermal )

Mean first passage time of free diffusion  $\tau = \frac{x^2}{6D}$

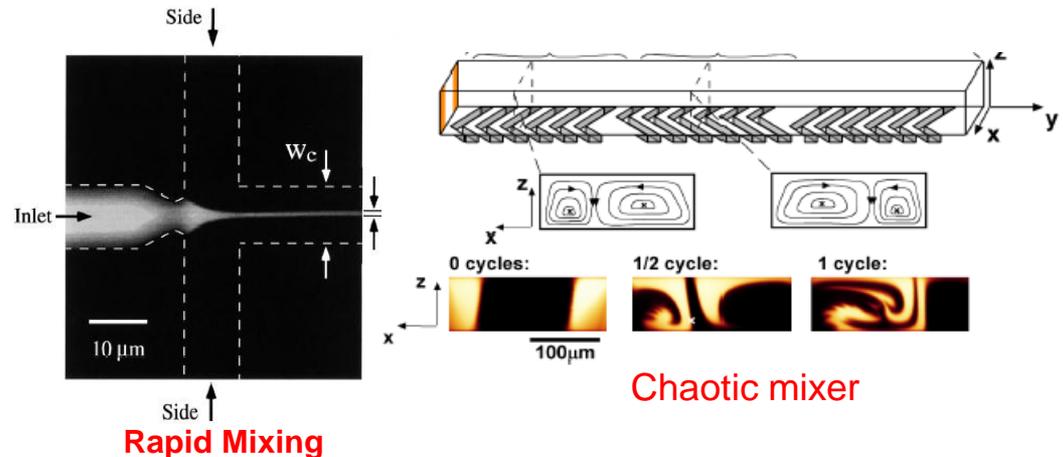
Einstein relation  $D = \frac{kT}{6\pi\mu r}$

$t_{\text{Diff}} \sim L^2$

- Diffusion time of a macromolecule with  $D$  of  $10^{-5} \text{ cm}^2/\text{s}$

Volume	1 $\mu\text{L}$	1 nL	1 pL	1 fL	1 aL
Length of cube side $x$	1 mm	100 $\mu\text{m}$	10 $\mu\text{m}$	1 $\mu\text{m}$	100 nm
Time to diffuse $x$	500 s	5 s	0.05 s	0.5 ms	0.05 ms

- Mixing at microscale mediated mainly by diffusion



# Scaling in a fluidic system / Dimensionless Numbers

## Scaling Reynolds number

$$\text{Re} = \frac{\text{Inertial force}}{\text{Viscous force}} \approx \frac{\rho L^3 \cdot dV / dt}{\mu \cdot (dV / dL) \cdot L^2} \approx \frac{\rho L^3 \cdot V / t}{\mu \cdot (V / L) \cdot L^2} \approx \frac{\rho L^3 \cdot V / (L / V)}{\mu \cdot (V / L) \cdot L^2}$$

$$\text{Re} = \frac{\rho \cdot V \cdot L}{\mu} \quad \sim L^2$$

$\rho$ : density of the fluid  
 $L$ : characteristic length  
 $V$ : velocity  
 $\mu$ : viscosity

Laminar flow

- Bacteria in water  $10^{-6}$
- Marble falling in honey  $10^{-2}$
- Tropical fish  $10^2$
- Dragonfly  $10^3$

Turbulent flow

- Car  $10^6$
- Airplane  $10^7$
- Whale  $10^8$

## ► Scaling Weber number

$$We = \frac{\text{Inertial force}}{\text{Surface tension force}} \approx \frac{\rho L^3 \cdot V / (L/V)}{\sigma \cdot L}$$

$$We = \frac{\rho \cdot V^2 \cdot L}{\sigma} \sim L^3$$

$\sigma$ : Surface tension

## ► Scaling Capillary number

$$Ca = \frac{\text{Viscous force}}{\text{Surface tension force}} \approx \frac{\mu \cdot (V/L) \cdot L^2}{\sigma \cdot L}$$

$$Ca = \frac{\mu \cdot V}{\sigma} \sim L$$

The surface tension force dominates over the viscous force in the micro- and nanoscale.

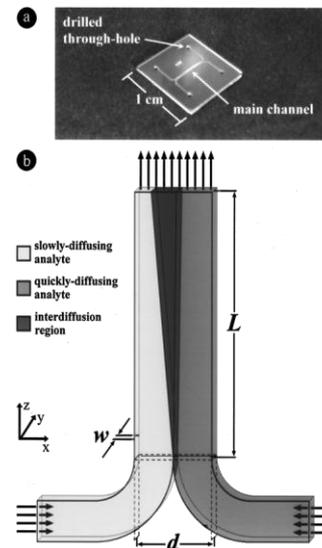
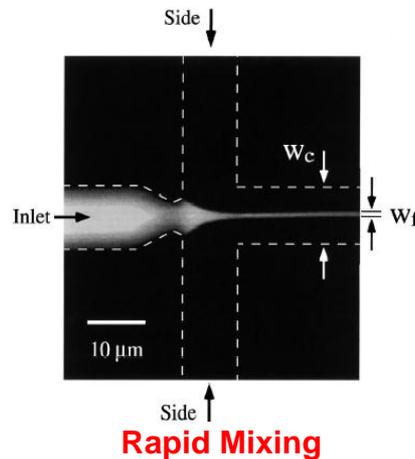
## ► Scaling Peclet number

$$Pe = \frac{\text{Convection}}{\text{Diffusion}} = \frac{\text{Diffusion time}}{\text{Convection time}} = \frac{L^2 / D}{L/V}$$

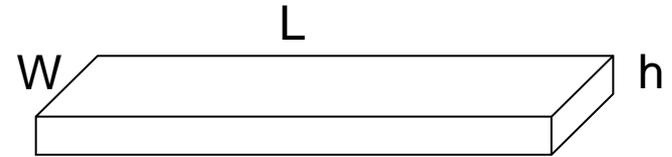
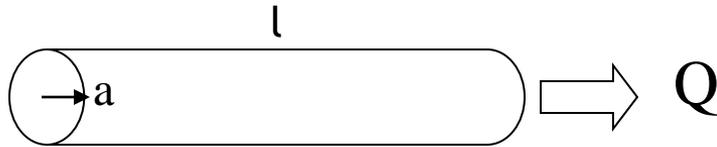
$$Pe = \frac{L \cdot V}{D} \sim L^2$$

$\sigma$ : Surface tension

The diffusion time may approach the order of the convection time. This fact leads to the possibility of real-time measurements of reaction kinetics



## ► Scaling in Pressure-pumping



Pressure drop  $\Delta P = \frac{8\mu l Q}{\pi a^4} \sim L^{-3}$

$\Delta P = \frac{12\mu L}{Wh^3} Q \sim L^{-3}$

e.g.



$\mu_{\text{water, 20 C}} = 11.3 \cdot 10^{-4} \text{ (Pa}\cdot\text{s)}$

•(W,h,L)= (100 μm, 30μm, 3cm), Q= 1 μl/min

$\Delta P = 1.5 \cdot 10^5 \text{ (Pa)} = 1.5 \text{ atm}$

•(W,h,L)= (100 μm, 0.3μm, 3cm), Q= 1 μl/min

$\Delta P = 1.5 \cdot 10^6 \text{ atm}$

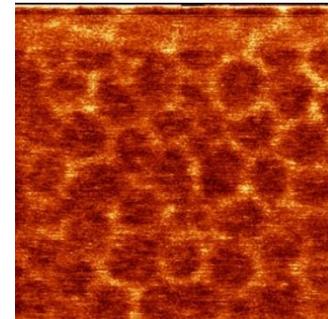
Pressure-driven pumping becomes very difficult !!

## ■ Scaling in color

- Bulk gold appears yellow in color
- Nanosized gold appears red in color
  - The particles are so small that electrons are not free to move about as in bulk gold
  - Because this movement is restricted, the particles react differently with light



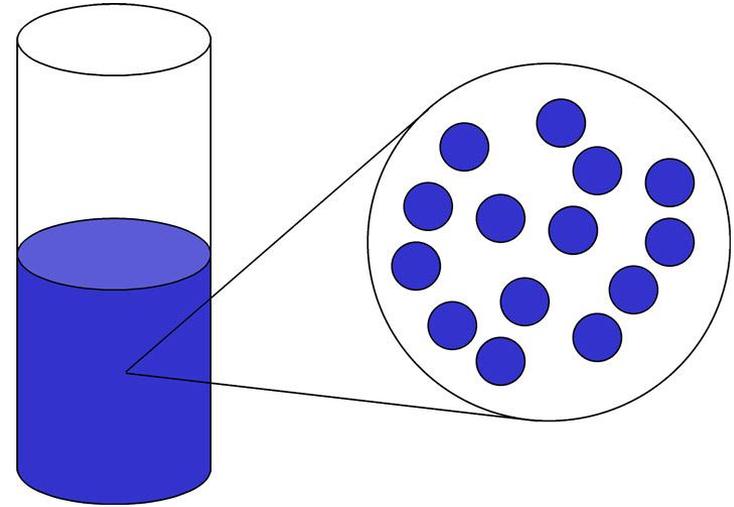
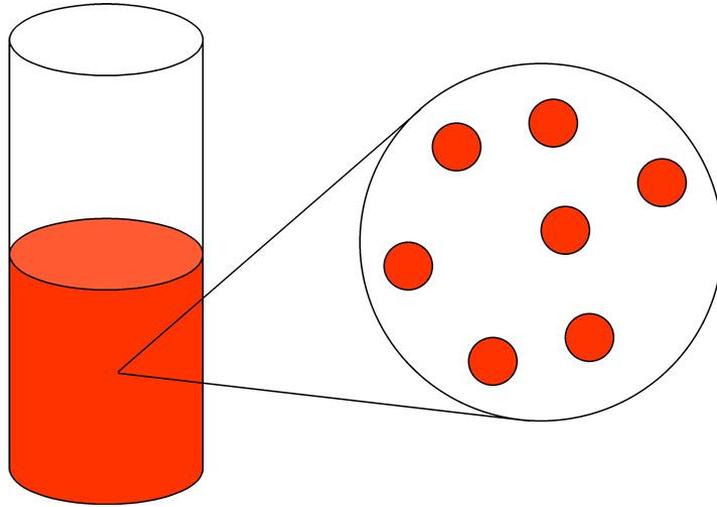
“Bulk” gold looks yellow



12 nanometer gold particles look red

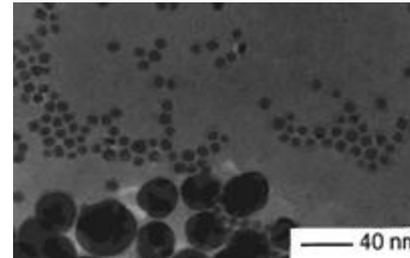
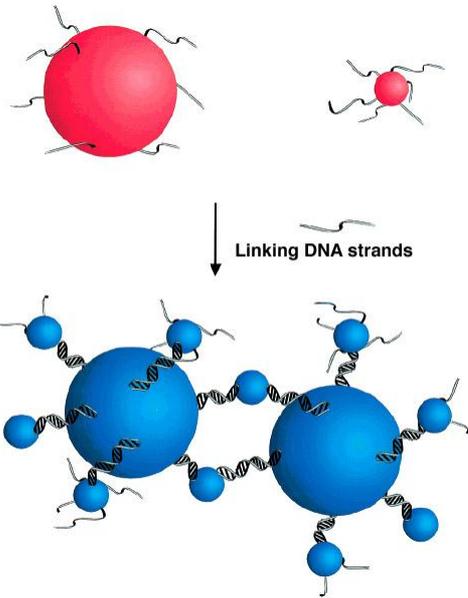
Sources: <http://www.sharps-jewellers.co.uk/rings/images/bien-hccncsq5.jpg>  
<http://www.foresight.org/Conferences/MNT7/Abstracts/Levi/>

# “Color change” of Au Nanoparticle

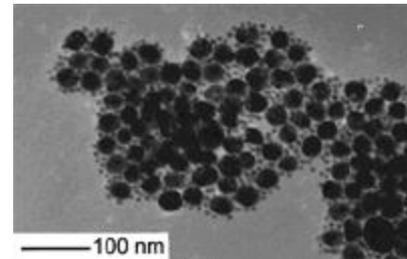
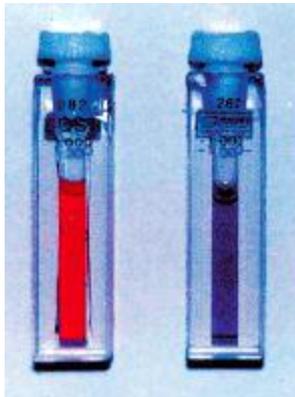


- Au nanoparticles suspend in solutions
- “Transparent”
- The color of particles comprised of 1,000-10,000 gold atoms depends on the **distance** between the particles.

# “Color change” of Au Nanoparticle



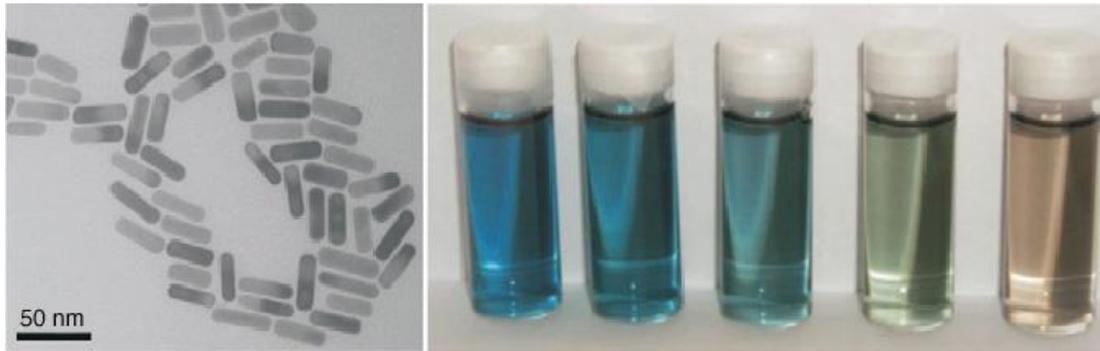
8 and 30 nm gold particles, no DNA link



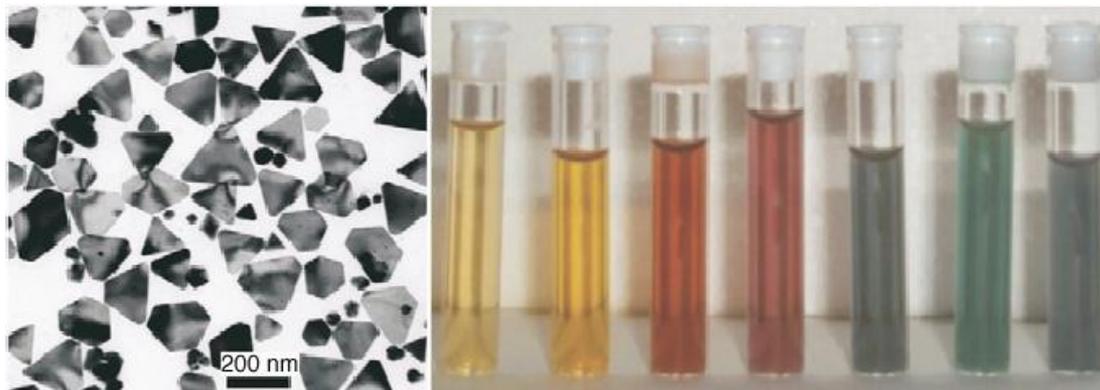
8 and 30 nm gold particles, DNA link

Chad A. Mirkin, *Inorg. Chem.* **2000**, *39*, 2258-2272

# “Color change” of Au Nanoparticle



Au nanorods of increasing aspect ratio



Ag nanoprisms with increasing lateral size

Optical properties of metal nanoparticles depend strongly on particle **size** and **shape** and **the distance to neighboring particles**. For Au, Ag, and Cu the collective oscillation of surface conduction electrons in response to the alternating electric field of incident light induces a quantized charge density wave (plasmon resonance) that absorbs some visible wavelengths.

# *Semiconductor Nanocrystals “Quantum Dots”*

## Optical Properties

- Broad excitation profile
- Narrow emission bandwidth
- Good photostability
- Higher emission intensity

